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Assistant Commissioner for Patents
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Sir:

Transmitted herewith for filing is the Patent Application (37 CFR 1.53(b)) in the name(s) of:
**Thomas WEYH, Ulrich SIMON, Guenter SCHOEPPPE, Ralf WOLLESCHENSKY
and Michael STOCK**

FOR: **ARRANGEMENT FOR ILLUMINATION AND/OR DETECTION IN A MICROSCOPE**

ENCLOSED ARE:

- 09295555 042199
- (X) 10 pages of Specification, 2 pages of Claims (# of claims 10) & Abstract;
 - (X) Figs. 1 - 10 / Eleven (11) sheet(s) of Drawings;
 - (X) Declaration and Power of Attorney;
 - (X) Assignment to: *Carl Zeiss Jena GmbH* ;
 - (X) Certified copy(ies) of *German Pat. Appli. No. 198 35 072.4 filed August 4, 1998*, the priority(ies) of which is(are) claimed under 35 USC 119;
 - () Verified Statement to establish Small Entity Status (37 CFR 1.9 & 1.27);
 - () Information Disclosure Statement, PTO-1449 and ___ reference(s);

THE FILING FEE HAS BEEN CALCULATED AS SHOWN BELOW:

	Claims filed		Extra	—SMALL \$ —380.00	LARGE \$ 760.00	AMOUNT \$ 760.00
Total Claims	10	Minus 20		x \$ —9.00	x \$ 18.00	\$.00
Independent	6	Minus 03	3	x \$ —39.00	x \$ 78.00	\$ 234.00
Multiple dependent claim fee				+ \$ —130.00	+ \$ 260.00	\$.00
Assignment recordation fee (\$ 40.00):						\$ 40.00
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The Commissioner is hereby authorized to charge any additional fees associated with the filing of this application but not limited to: (X) Any patent application processing fees under 37 CFR 1.17
(X) Any filing fees under 37 CFR 1.16 for the presentation of extra claims
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Respectfully submitted

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GHK:ram

ARRANGEMENT FOR ILLUMINATION AND/OR DETECTION IN A MICROSCOPEBACKGROUND OF THE INVENTIONa) Field of the Invention

5 The invention is directed to a laser scanning microscope comprising a laser unit, scanning means, a microscope stand, a detection unit and a control/receiving unit, wherein the spectral characteristics of the detection unit can be freely programmed by a switching mirror array integrated in a monochromator. The switching mirror array (one- or two-dimensional) can be constructed, for example, as a DMD (Digital Mirror Device or switchable -mirror arrangement). The laser scanning microscope according to the invention enables different operating modes. On the one hand, the emitted spectrum can be detected with high resolution on every scanned pixel (in the specimen); on the other hand, the emitted spectrum can be divided into a quantity of spectral portions (zones on the switching mirror array) and each of these portions can be treated as a separate electronic detection channel (which is advantageous, e.g., for receiving multiple fluorescences). Further, a freely programmable confocal diaphragm (pinhole) can be realized by means of an additional switching mirror array which is introduced in a conjugate plane to the object plane.

b) Description of the Related Art

20 Modern laser scanning microscopes for examination of (fluorescing) specimens generally comprise a detection unit which divides the (fluorescent) radiation emitted from the specimen into a certain quantity of (generally up to 4) detection channels by means of dichroic splitter layers and filter layers (principle of optical multichannel analyzer - OMA). These splitters/filters are generally held in
25 rotatable revolving wheels or linear-displaceable disks. In this way, a spectral adaptation of the channels to the spectral characteristics of the specimen radiation is possible up to a certain degree. However, since only a finite number of dielectric

splitters and filters can be received in every holder and the spectral characteristics of every individual splitter/filter are determined in the process of their manufacture, this arrangement is not flexible enough to be adapted to the specimen spectrum in an optimum manner in many cases of application (Fig. 1).

5 A confocal microscope with DMD mirror arrays for illumination and/or detection is described in U.S. Patent 5,587,832.

OBJECT AND SUMMARY OF THE INVENTION

The primary object of the invention is a laser scanning microscope which is substantially more flexible with respect to its excitation and/or detection.

10 The invention encompasses a laser scanning microscope with a detection unit whose spectral characteristics are freely programmable by means of a switching mirror array integrated in a monochromator.

15 This laser scanning microscope, according to the invention, comprises a laser unit, scanning means, a microscope stand, a detection unit and a control/receiving unit. The (fluorescent) radiation which is emitted from the specimen can be focused (in the case of confocal applications) on a confocal pinhole that is positioned in a conjugate object plane. This pinhole then simultaneously represents the entrance aperture of a (grating) monochromator which divides the specimen radiation into its spectral components through its
20 dispersive effect. An at least one-dimensional switching mirror array on which the specimen spectrum is optically imaged (Fig. 2) is located in the focal plane of the dispersive medium (grating).

25 The at least one-dimensional switching mirror array comprises a quantity of individually controllable switching mirrors. While the scanning means essentially dwell on one specimen point, one mirror after the other can now be individually controlled (and therefore switched), e.g., sequentially, and the individual spectral components of the specimen radiation are accordingly reflected onto a suitably synchronized detector sequentially for reception of the entire spectrum.

30 Alternatively, adjacent mirror zones corresponding to whole spectral bands can be controlled in parallel in order to simultaneously detect entire

frequency bands in this way (one band after the other or a plurality of bands simultaneously). In the case of fluorescent radiation, those mirror pixels that correspond to the excitation radiation can advantageously be omitted from the detected spectrum.

5 In a variant, the excitation radiation can advantageously be coupled into the system via the mirror pixels corresponding to the excitation (Figs. 3a, b). The need for a main beam splitter (DBS) is therefore circumvented and an appreciably more compact system construction can be realized. In addition, the excitation radiation in this case automatically passes through the detection pinhole as illumination pinhole, which leads to an improvement in beam quality (spatial filtering) and therefore improved spatial resolution of the entire microscope system. In addition, by means of oscillating the mirror utilized for reflecting the excitation radiation between two possible mirror positions, the illumination intensity can be adjusted in an almost continuous manner and can be changed in a synchronized manner with respect to the scan pixels (shading compensation, intensity modulation, etc.).

10 Further, a freely programmable confocal diaphragm (pinhole) can be realized (Fig. 4) by means of another switching mirror array which is introduced in a conjugate plane to the object plane. This pinhole is freely programmable with respect to shape and size (adjustable confocal volume) as well as with respect to lateral position, which increases the flexibility of the system and is a great advantage for the adjustment of the optical system (autoadjustment of pinhole). In addition, in multichannel applications, the pinhole size can be synchronized with the spectral band detected at that instant in order that optical sections independent from the wavelength can be realized with the confocal microscope. In addition, the pinhole size can also be advantageously adapted to the intensity of the fluorescent radiation when various fluorescences of very different intensity are present simultaneously in the specimen and are to be detected.

20 In an advantageous variant, a curved grating can be used, which curved grating likewise takes over the collimation and the dispersion of the radiation to be detected and accordingly results in a reduced quantity of optical components

(Fig. 5). The structural size of the arrangement according to the invention in its entirety is accordingly advantageously reduced. Above all, this leads to a greater optical stability of the detection system.

In a variant, the optical grating can be replaced by a prism. In this way, an increase in the efficiency of the optical system is potentially possible (Fig. 6), particularly in the detection of unpolarized light.

In a variant, the spectroscopic system can also be adapted to an existing state-of-the-art laser scanning microscope in order to carry out a spectral characterization of the emission radiation of the microscopic specimen. This can be carried out in particular via a fiber coupling of the spectrometric unit to the laser scanning microscope, wherein the fiber can be arranged, for example, directly behind one of the confocal pinholes (Fig. 7).

In a variant which has as subject matter the excitation of multiphoton fluorescence, a confocal diaphragm can be entirely dispensed with due to the three-dimensionally spatially resolved excitation (Fig. 8). In this case, in the arrangement according to the invention, the confocal diaphragm in the monochromator entrance diaphragm plane can be omitted and the emission light can be radiated directly onto the dispersive medium.

In fluorescence microscopy, application in the biomedical field is generally concentrated in the wavelength band from approximately 350 to 800 nm. The wavelength resolution required for application lies in the range of about 0.5 nm. At the present time, switching mirror arrays can be obtained (also commercially) in a wide variety of constructions (e.g., from Texas Instruments, Inc., Dallas, TX), also, for example, in 576 x 864 pixel² display form. Accordingly, when imaging the spectrum along the 864 pixels, a resolution of about 0.5 nm can be realized. The individual mirrors can be switched in a digitally controlled manner between two highly-stable positions ($\pm 10^\circ$), wherein the switching process is concluded within approximately 300 ns. The reflecting mirrors can be digitally programmed optionally and independently from one another.

Gratings, prisms or combinations thereof, for example, can be used as dispersive media in the constructions described above. By using these components

in a double-pass configuration, the effective dispersion can be doubled and a particularly compact construction of the laser scanning microscope can accordingly realized in an advantageous manner.

In principle, all of the arrangements described herein can also be realized in transmission mode by using a transmission array (LCD array; liquid crystal) instead of the switching mirror array (Fig. 9).

A line-scanning laser scanning microscope can be realized in that the laser beam is expanded to a line and scanned over the object by means of only one scanner (one scanning axis) (Fig. 10). When the punctiform pinhole in Figure 2 is replaced with a slit pinhole along the line-shaped laser beam, the DMD is replaced by a two-dimensional switching mirror array and the detector is replaced by a (sensitivity-enhanced) CCD, the system can be operated in line scanning mode. The scanned line is imaged in one dimension of the DMD array and the spectrum of this object line is imaged in the other coordinate.

The resolving capacity of the spectrometric system can be adapted to the needs of the application in question by exchanging the optical grating or by displacing and rotating the grating (monochromator size)

BRIEF DESCRIPTION OF THE DRAWINGS

In the drawings:

Fig. 1 is a schematic representation of a microscope M and scan head S and which form an LSM;

Fig. 2 shows, also in schematic form, a further embodiment of the laser scanning microscope in accordance with the invention;

Figs. 3a and 3b are optical arrangements indicating how the excitation radiation can be coupled into the system in accordance with the invention;

Fig. 4 illustrates in schematic representation how a freely programmable diaphragm (pinhole) can be realized instead of PH1 in Fig. 2;

Fig. 5 is a schematically represented further embodiment using a curved grating;

Fig. 6, in another schematically represented embodiment, uses a prism instead of the optical grating;

Fig. 7 is a schematically represented embodiment which employs an additional fiber for carrying out a spectral characterization of the emission radiation of the microscopic specimen;

Fig. 8, also in schematic representation, shows an arrangement in accordance with the invention in which the confocal diaphragm as in Fig. 2 can be dispensed with;

Fig. 9 further schematically shows an arrangement as in Fig. 2 but which includes a transmissive modulator which passes only the relevant wavelength of the dispersed spectrum; and

Fig. 10 shows in schematic representation how a line scanning laser scanning microscope can be realized.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

Fig. 1 shows schematically a microscope unit M and a scan head S which have a common optical interface via an intermediate image and form an LSM.

The scan head S can be mounted on the phototube of an upright microscope as well as on a lateral output of an inverse microscope.

The drawings show a microscope beam path which is switchable between incident light scanning and transmitted light scanning by means of a swivelable mirror 14, with a light source 1, illumination optics 2, beam splitter 3, objective 4, specimen stage 5, condenser 6, light source 7, receiver arrangement 8, a tube lens 9, an observation beam path with a tube lens 10 and an eyepiece 11, and a beam splitter/mirror 12 for coupling in the scanning beam. A laser module 13.1, 13.2 holds the laser and is connected via monomode light-conducting fibers 14.1, 14.2 with the laser input coupling unit of the scan head S.

The coupling of radiation into the light-conducting fibers 14.1, 14.2 is carried out by displaceable collimating optics and beam deflecting elements 17.1, 17.2. A monitoring beam path is stopped down by means of a partially reflecting mirror 18 in the direction of a monitor diode 19, wherein line filters 21 and neutral

filters 20 are advantageously arranged in front of the monitor diode 19 on a rotatable filter wheel, not shown.

The actual scan unit comprises a scanning objective 22, X/Y scanner 23, main beam splitter 24 and common imaging optics 25 for detection channels 26.1 - 26.4.

A deflecting prism 27 arranged behind the imaging optics 25 reflects the radiation coming from the object 5 in the direction of dichroic beam splitters 28 in the convergent beam path of the imaging optics 25, wherein pinholes 29 which are displaceable in the direction of and vertical to the optical axis and which are adjustable in diameter are arranged along with emission filters 30 and suitable receiver elements 31 (PMT) individually for each detection channel following the beam splitters 28.

A control unit/computer unit 34 is connected, among others, with the stage 5 and the scanners 23 and controls them.

Fig. 2 shows a possible embodiment form of the laser scanning microscope, according to the invention, comprising a laser unit L followed by shutter S, collimation optics KO, beam splitter ST1 for the output coupling of a monitor beam path MO, a beam splitter ST2 for conducting into scanning means SC and in the direction of detection, a microscope analogous to Fig. 1, with additional detection DT1 outside of the scanning beam path, wherein mirror 12 is constructed in this case as a beam splitter, a detection unit and a control/receiving unit. The radiation emitted from the specimen can (in confocal applications) be focused on a confocal pinhole PH1 positioned in a conjugate object plane. This pinhole PH1 then simultaneously forms the entrance aperture of a (for example, grating GT and imaging mirrors SP1, SP2) monochromator which divides the specimen radiation into its spectral components through its dispersive effect. An at least one-dimensional switching mirror array DMD1 on which the specimen spectrum is optically imaged is located in the focal plane of the dispersive medium (for example, grating), wherein focusing optics FO and a detector DT3 are arranged following the one-dimensional switching mirror array DMD1.

Figs. 3a,b: In an advantageous construction, the excitation radiation can advantageously be coupled into the system via the mirror pixels which correspond to the excitation. Accordingly, the need for a main beam splitter (DBS) is circumvented and an appreciably more compact system construction can be realized. In addition, the excitation radiation in this case automatically passes through the detection pinhole as illumination pinhole, which leads to an improvement in the beam quality (spatial filtering) and therefore leads to an improved spatial resolution of the entire microscope system. In addition, in that the mirror utilized for reflecting the excitation radiation is oscillated between two possible mirror positions, the illumination intensity can be adjusted in an almost continuous manner and can be changed in a synchronized manner with respect to the scan pixels (shading compensation, intensity modulation, etc.). A light-coupling fiber F is shown schematically in Fig. 3a.

The coupled in laser light (in) reaches a grating GT2, is spectrally divided and is reflected on a DMD arrangement, shown schematically by a line extending along the dispersion direction, via a field lens FL1 for parallelizing.

Through selective switching of individual mirror elements, shown schematically with reference to Fig. 3b, determined wavelengths or wavelength areas (excitation light) are reflected back in the ON position in the direction of the grating, while others, in the off position of the mirror, do not travel back to the grating GT2 and are selected.

For the wavelength components (excitation light) reflected back to the grating GT2, the dispersion is eliminated again and they are imaged on a pinhole PH2 in the input of the microscope (out-on) since they impinge on the grating in an offset manner.

The light returning from the object passes through PH2, GT2, FL1, DMD, an additional field lens FL2 in the direction of a detection unit DE shown schematically.

Reflection is carried out in a wavelength-selective manner (out-off) in the direction of detection in the OFF position.

Splitting into individual wavelengths is carried out at the grating GT2 and these individual wavelengths can be detected individually.

Fig. 4: A freely programmable confocal diaphragm (pinhole) can be realized instead of PH1 in Fig. 2 by means of another switching mirror array DMD1 which is introduced in a conjugate plane to the object plane. This pinhole is freely programmable with respect to shape and size (adjustable confocal volume) as well as with respect to lateral position, which increases the flexibility of the system and is a great advantage for the adjustment of the optical system (autoadjustment of pinhole). In addition, in multichannel applications, the pinhole size can be synchronized with the spectral band detected at that instant in order that optical sections independent from the wavelength can be realized with the confocal microscope. In addition, the pinhole size can also be advantageously adapted to the intensity of the fluorescent radiation when various fluorescences of very different intensity are present simultaneously in the specimen and are to be detected.

Fig. 5: In a variant, a curved grating GT3 can be used, which likewise takes over the collimation and the dispersion of the radiation to be detected and accordingly results in a smaller quantity of optical components by doing away with the imaging mirrors SP1, SP2 in Fig. 2. The structural size of the arrangement according to the invention in its entirety is accordingly advantageously reduced. This results, above all, in a greater optical stability of the detection system.

Fig. 6: In another embodiment form, the optical grating can also be replaced by a prism P. In this way, an increase in the efficiency of the optical system is potentially possible, particularly in the detection of unpolarized light.

Fig. 7 shows a state-of-the-art laser scanning microscope similar to Fig. 1, without reference numbers in this case, at which, by means of an additional fiber F1, a possible embodiment form of the spectroscopic detection system according to the invention as described, for example, in Fig. 5 is coupled out of one of the detection beam paths (26.1 in Fig. 1) directly following the pinhole in order to carry out a spectral characterization of the emission radiation of the microscopic specimen.

Fig. 8: In the case of excitation of multiphoton fluorescence, in the arrangement according to the invention, the confocal diaphragm (PH1 in Fig. 2, DMD1 in Fig. 4) in the monochromator entrance diaphragm plane can be dispensed with and the emission light can be radiated directly onto the dispersive medium as is shown with reference to the arrangement with curved mirror according to Fig. 5.

Fig. 9 shows a further construction as in Fig. 2, but which has, instead of the DMD following the grating GT1, a transmissive modulator MT, for example, of an LCD array, which passes only the relevant wavelengths of the dispersed spectrum to the detector.

A construction of an LCD array instead of a pinhole analogous to the DMD in Fig. 4 in a transmission beam path is also possible in an advantageous manner.

Fig. 10 shows that a line-scanning laser scanning microscope can be realized in that the laser beam is expanded on a line, for example, with a cylinder lens, and scanned over the object by means of only one scanner (one scanning axis), for example, in the Y-direction in this case. When the punctiform pinhole in Fig. 2 is replaced with a slit pinhole along the line-shaped laser beam which is realized by means of a two-dimensional switching mirror array DMD1, represented by the dark mirrors in the shape of a stripe, and the detector is replaced by a (sensitivity-enhanced) CCD, the system can be operated in line scanning mode. The scanned line is imaged in one dimension of the DMD array and the spectrum of this object line is imaged in the other coordinate.

While the foregoing description and drawings represent the preferred embodiments of the present invention, it will be obvious to those skilled in the art that various changes and modifications may be made therein without departing from the true spirit and scope of the present invention.

What is claimed is:

1 1. A laser scanning microscope comprising:
2 at least one selectively switchable micro-mirror arrangement in at least
3 one of the illumination beam path and detection beam path which is used for the
4 wavelength selection of at least one of dispersively divided illumination and object
5 light such as reflection, fluorescence.

1 2. A combination comprising:
2 at least one micro-mirror arrangement with at least one dispersion
3 element for wavelength-selective coupling in of illumination light in the direction of
4 the object and wavelength-selective coupling out of object light in the direction of
5 detection in a microscope.

1 3. A method of using the combination as in claim 2 comprising the
2 step of using said combination in a laser scanning microscope.

1 4. An arrangement according to claim 1 further comprising at least
2 one grating and prism as dispersive element.

1 5. In a laser scanning microscope, an arrangement of a micro-
2 mirror arrangement for use instead of a confocal pinhole diaphragm in the detection
3 beam path.

1 6. In a laser scanning microscope, an arrangement of an LCD
2 arrangement for use instead of a confocal pinhole diaphragm in the detection beam
3 path.

1 7 An optical connection of an arrangement according to claim 1,
2 the detection beam path comprising dichroic beam splitters for splitting the
3 detection beam path into individual channels.

1 8. The arrangement according to claim 7, wherein the optical
2 connection is carried out via light-conducting fibers.

1 9. In a laser scanning microscope with slit-shaped scanning in at
2 least one direction comprising:
3 at least one switchable micro-mirror arrangement; and
4 means for switching said at least one switchable micro-mirror
5 arrangement to provide said slit-shaped scanning.

1 10. In a laser microscope, a combination comprising at least one
2 dispersive element with a selectively switchable transmission diaphragm in a
3 detection beam path.

ABSTRACT OF THE DISCLOSURE

A laser scanning microscope comprises at least one selectively switchable micro-mirror arrangement (DMD) in the illumination beam path and/or detection beam path which is used for the wavelength selection of dispersively divided illumination and/or object light such as reflection, fluorescence.

5

50 51 52 53 54 55 56 57 58 59 60 61 62 63 64 65 66 67 68 69 70 71 72 73 74 75 76 77 78 79 80 81 82 83 84 85 86 87 88 89 90 91 92 93 94 95 96 97 98 99 100 101 102 103 104 105 106 107 108 109 110 111 112 113 114 115 116 117 118 119 120 121 122 123 124 125 126 127 128 129 130 131 132 133 134 135 136 137 138 139 140 141 142 143 144 145 146 147 148 149 150 151 152 153 154 155 156 157 158 159 160 161 162 163 164 165 166 167 168 169 170 171 172 173 174 175 176 177 178 179 180 181 182 183 184 185 186 187 188 189 190 191 192 193 194 195 196 197 198 199 200 201 202 203 204 205 206 207 208 209 210 211 212 213 214 215 216 217 218 219 220 221 222 223 224 225 226 227 228 229 230 231 232 233 234 235 236 237 238 239 240 241 242 243 244 245 246 247 248 249 250 251 252 253 254 255 256 257 258 259 260 261 262 263 264 265 266 267 268 269 270 271 272 273 274 275 276 277 278 279 280 281 282 283 284 285 286 287 288 289 290 291 292 293 294 295 296 297 298 299 300 301 302 303 304 305 306 307 308 309 310 311 312 313 314 315 316 317 318 319 320 321 322 323 324 325 326 327 328 329 330 331 332 333 334 335 336 337 338 339 340 341 342 343 344 345 346 347 348 349 350 351 352 353 354 355 356 357 358 359 360 361 362 363 364 365 366 367 368 369 370 371 372 373 374 375 376 377 378 379 380 381 382 383 384 385 386 387 388 389 390 391 392 393 394 395 396 397 398 399 400 401 402 403 404 405 406 407 408 409 410 411 412 413 414 415 416 417 418 419 420 421 422 423 424 425 426 427 428 429 430 431 432 433 434 435 436 437 438 439 440 441 442 443 444 445 446 447 448 449 450 451 452 453 454 455 456 457 458 459 460 461 462 463 464 465 466 467 468 469 470 471 472 473 474 475 476 477 478 479 480 481 482 483 484 485 486 487 488 489 490 491 492 493 494 495 496 497 498 499 500 501 502 503 504 505 506 507 508 509 510 511 512 513 514 515 516 517 518 519 520 521 522 523 524 525 526 527 528 529 530 531 532 533 534 535 536 537 538 539 540 541 542 543 544 545 546 547 548 549 550 551 552 553 554 555 556 557 558 559 560 561 562 563 564 565 566 567 568 569 570 571 572 573 574 575 576 577 578 579 580 581 582 583 584 585 586 587 588 589 590 591 592 593 594 595 596 597 598 599 600 601 602 603 604 605 606 607 608 609 610 611 612 613 614 615 616 617 618 619 620 621 622 623 624 625 626 627 628 629 630 631 632 633 634 635 636 637 638 639 640 641 642 643 644 645 646 647 648 649 650 651 652 653 654 655 656 657 658 659 660 661 662 663 664 665 666 667 668 669 670 671 672 673 674 675 676 677 678 679 680 681 682 683 684 685 686 687 688 689 690 691 692 693 694 695 696 697 698 699 700 701 702 703 704 705 706 707 708 709 710 711 712 713 714 715 716 717 718 719 720 721 722 723 724 725 726 727 728 729 730 731 732 733 734 735 736 737 738 739 740 741 742 743 744 745 746 747 748 749 750 751 752 753 754 755 756 757 758 759 760 761 762 763 764 765 766 767 768 769 770 771 772 773 774 775 776 777 778 779 780 781 782 783 784 785 786 787 788 789 790 791 792 793 794 795 796 797 798 799 800 801 802 803 804 805 806 807 808 809 810 811 812 813 814 815 816 817 818 819 820 821 822 823 824 825 826 827 828 829 830 831 832 833 834 835 836 837 838 839 840 841 842 843 844 845 846 847 848 849 850 851 852 853 854 855 856 857 858 859 860 861 862 863 864 865 866 867 868 869 870 871 872 873 874 875 876 877 878 879 880 881 882 883 884 885 886 887 888 889 890 891 892 893 894 895 896 897 898 899 900 901 902 903 904 905 906 907 908 909 910 911 912 913 914 915 916 917 918 919 920 921 922 923 924 925 926 927 928 929 930 931 932 933 934 935 936 937 938 939 940 941 942 943 944 945 946 947 948 949 950 951 952 953 954 955 956 957 958 959 960 961 962 963 964 965 966 967 968 969 970 971 972 973 974 975 976 977 978 979 980 981 982 983 984 985 986 987 988 989 990 991 992 993 994 995 996 997 998 999 1000

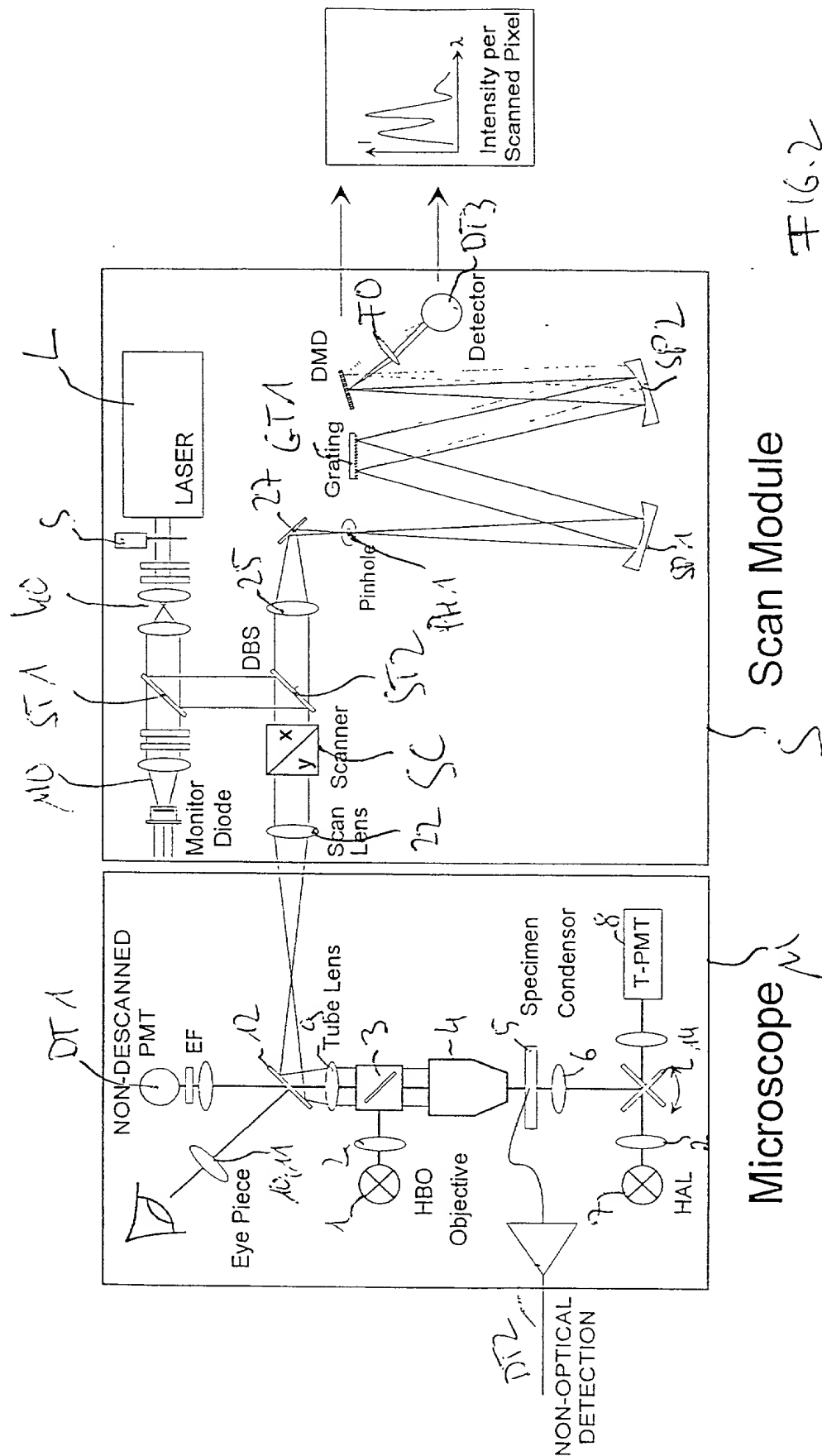


FIG. 2

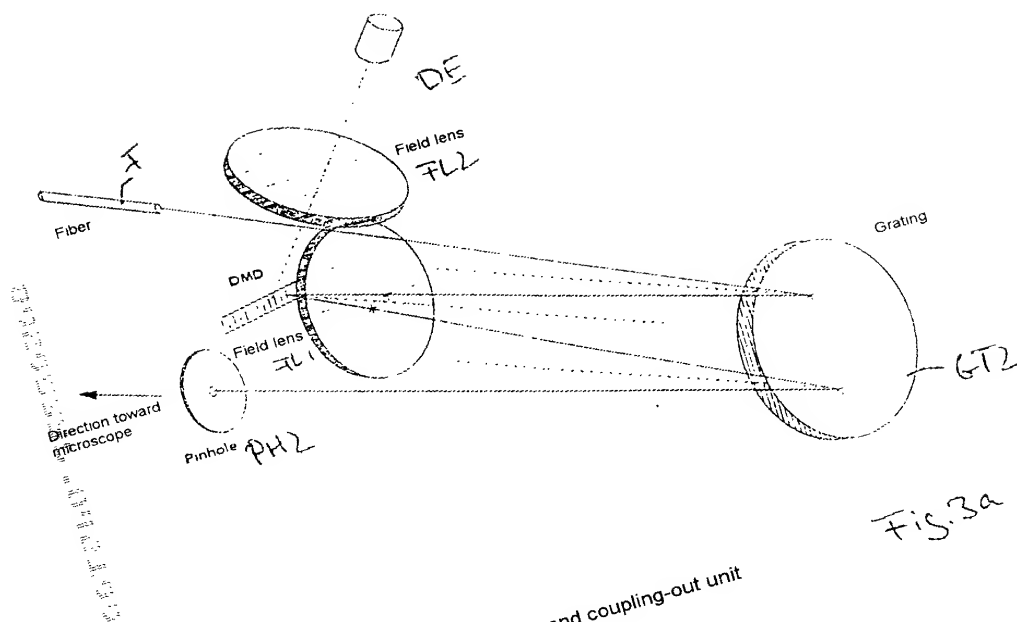
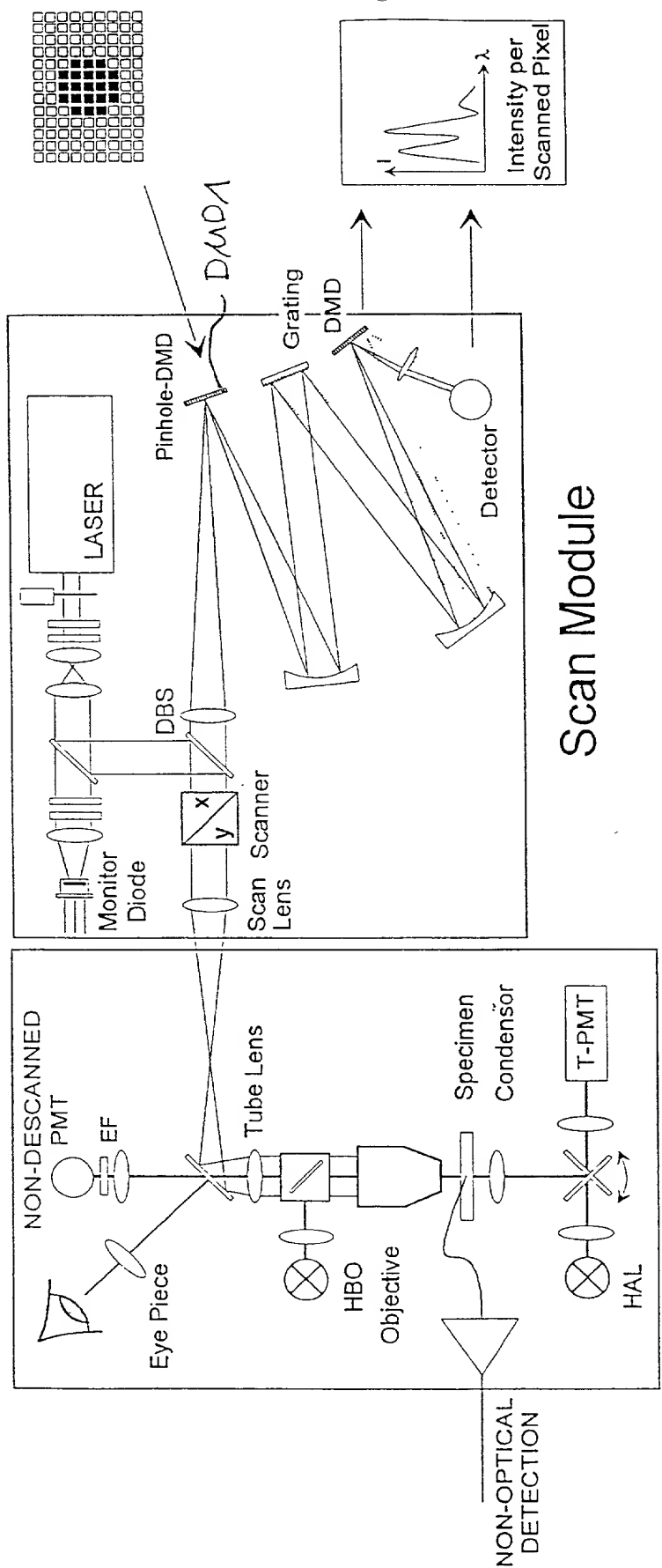


Fig. 3a

Freely programmable coupling-in and coupling-out unit



Microscope

Fig. 4.

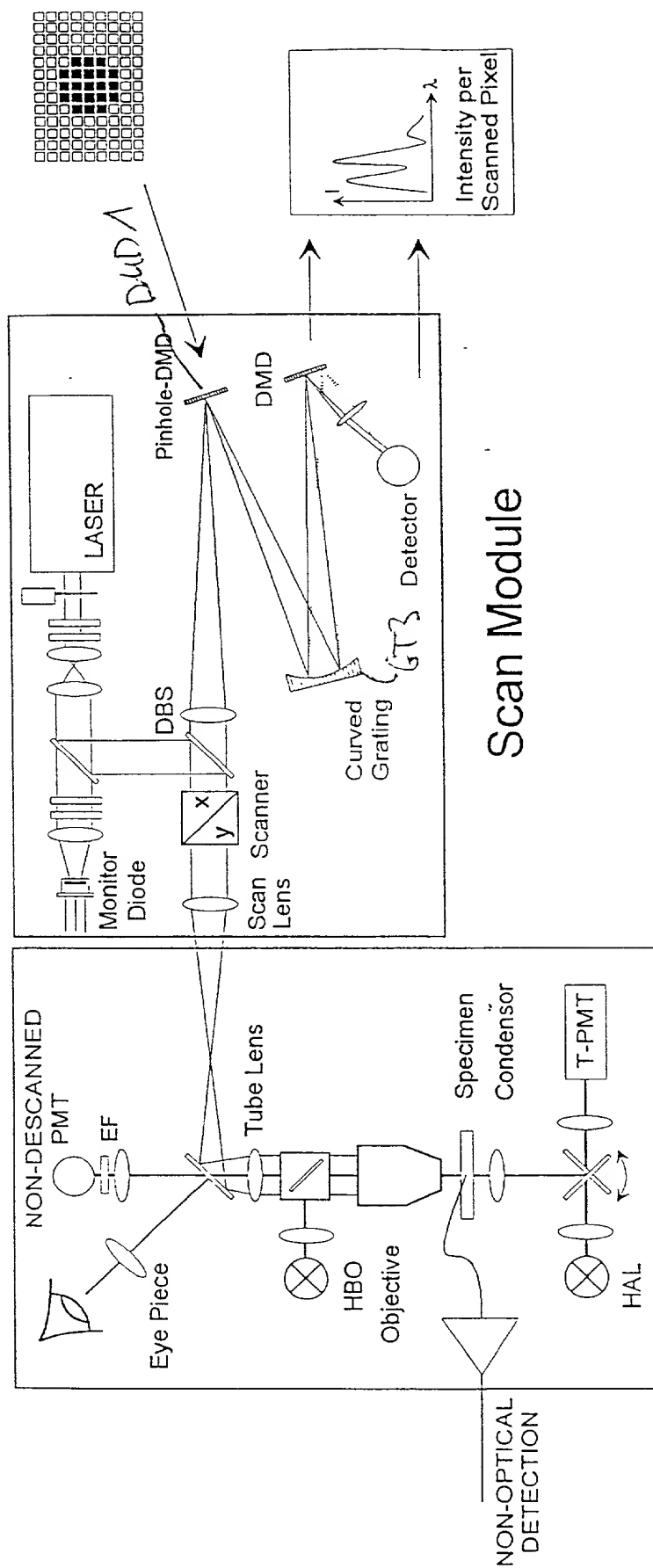


Fig. 5

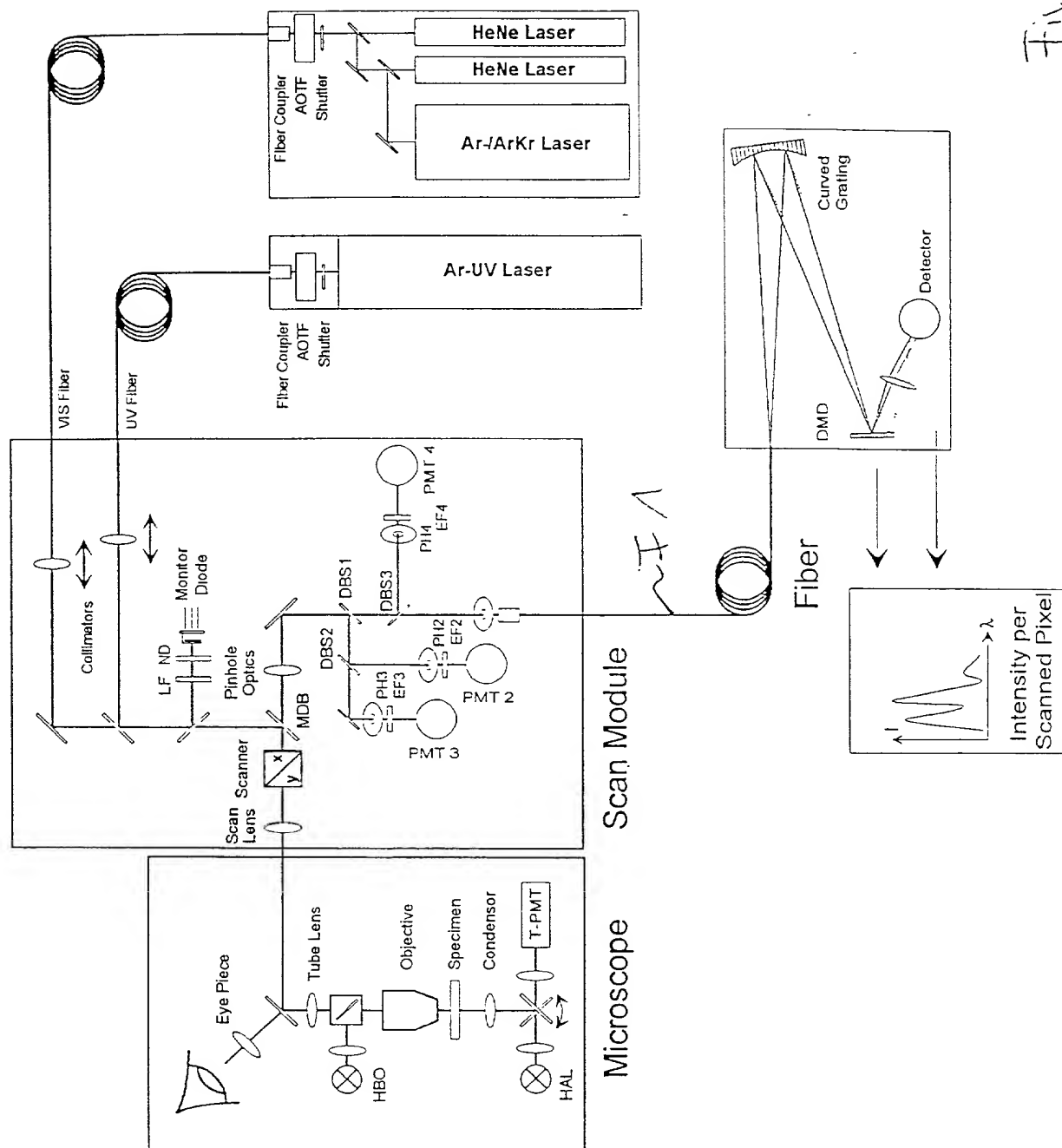


Fig 7.

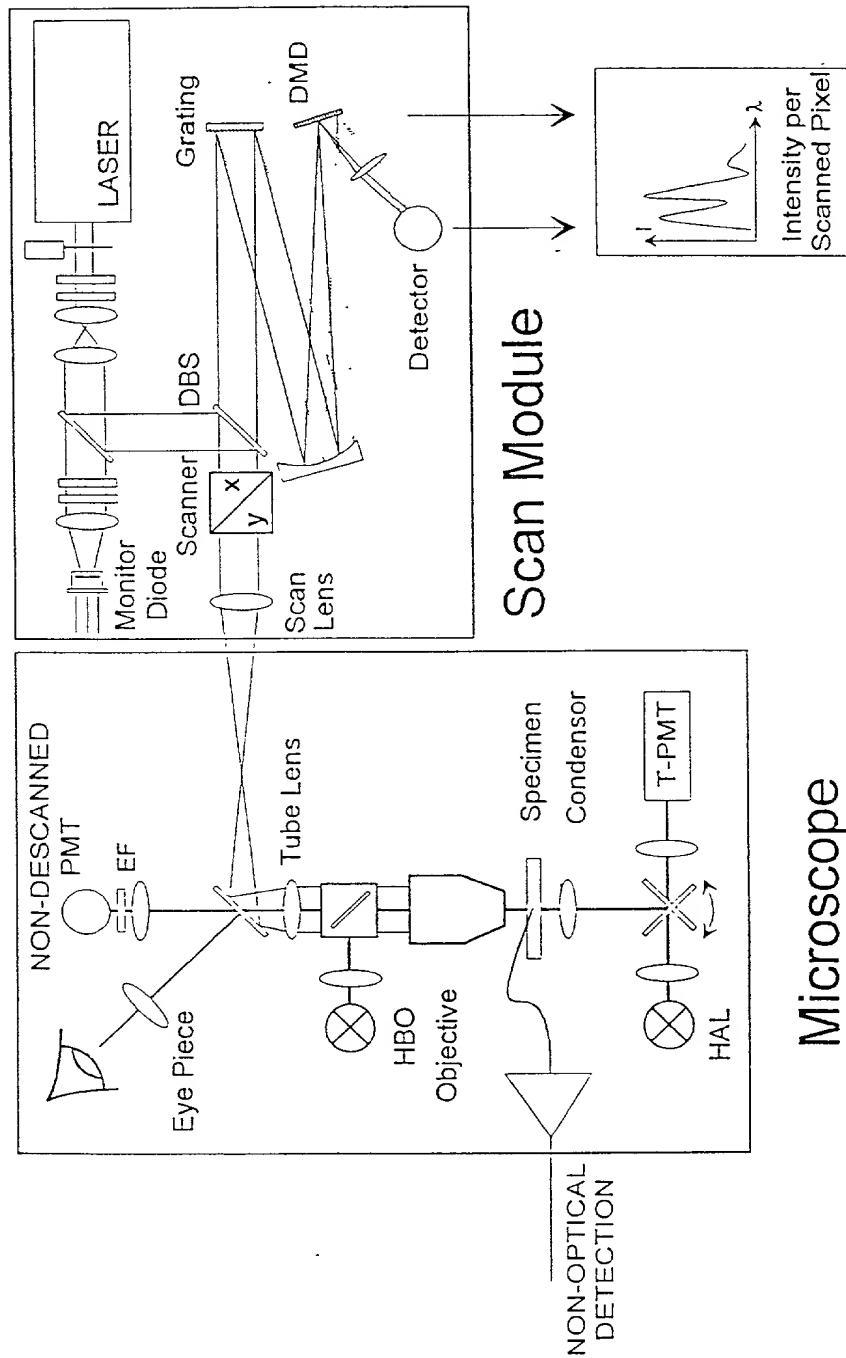
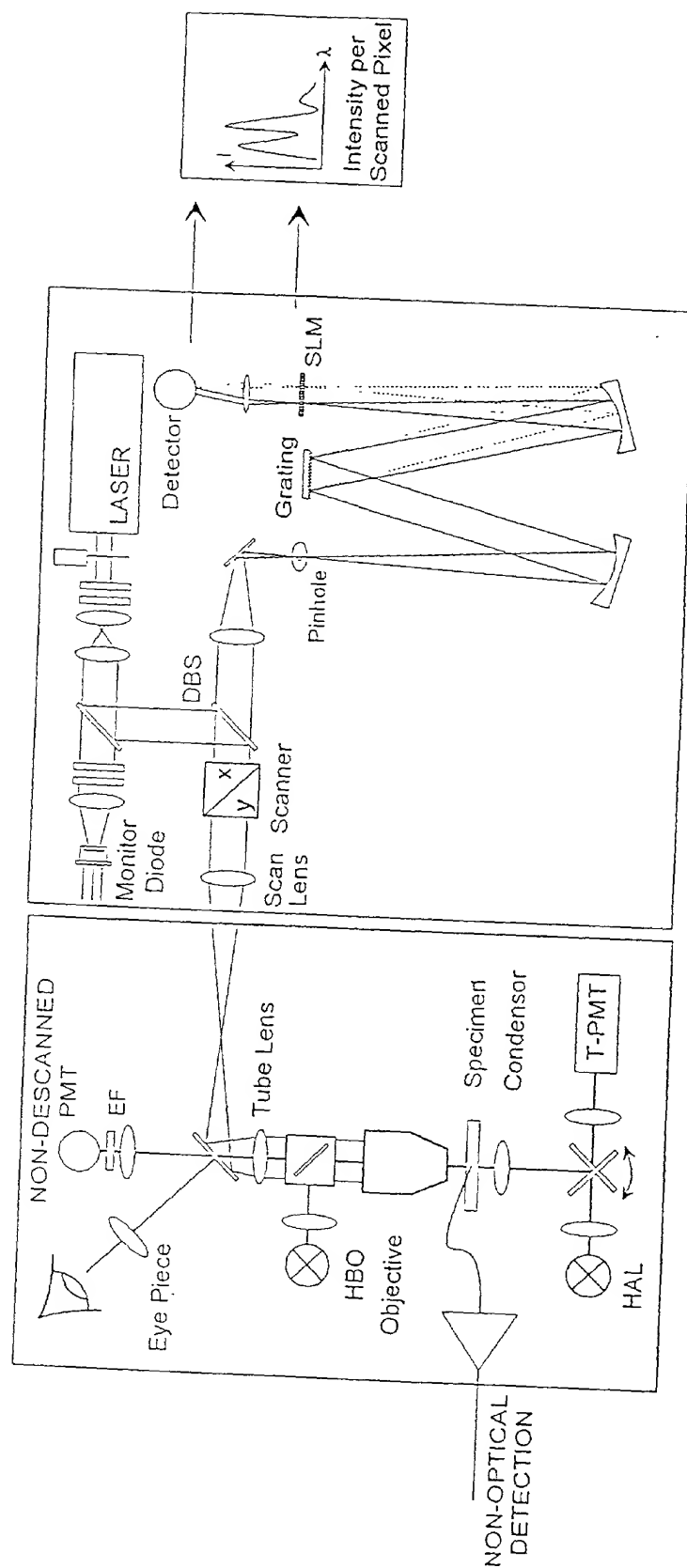


Fig. 8:

12345678910111213141516171819202122232425262728293031323334353637383940414243444546474849505152535455565758596061626364656667686970717273747576777879808182838485868788899091929394959697989910010110210310410510610710810911011111211311411511611711811912012112212312412512612712812913013113213313413513613713813914014114214314414514614714814915015115215315415515615715815916016116216316416516616716816917017117217317417517617717817918018118218318418518618718818919019119219319419519619719819920020120220320420520620720820921021121221321421521621721821922022122222322422522622722822923023123223323423523623723823924024124224324424524624724824925025125225325425525625725825926026126226326426526626726826927027127227327427527627727827928028128228328428528628728828929029129229329429529629729829930030130230330430530630730830931031131231331431531631731831932032132232332432532632732832933033133233333433533633733833934034134234334434534634734834935035135235335435535635735835936036136236336436536636736836937037137237337437537637737837938038138238338438538638738838939039139239339439539639739839940040140240340440540640740840941041141241341441541641741841942042142242342442542642742842943043143243343443543643743843944044144244344444544644744844945045145245345445545645745845946046146246346446546646746846947047147247347447547647747847948048148248348448548648748848949049149249349449549649749849950050150250350450550650750850951051151251351451551651751851952052152252352452552652752852953053153253353453553653753853954054154254354454554654754854955055155255355455555655755855956056156256356456556656756856957057157257357457557657757857958058158258358458558658758858959059159259359459559659759859960060160260360460560660760860961061161261361461561661761861962062162262362462562662762862963063163263363463563663763863964064164264364464564664764864965065165265365465565665765865966066166266366466566666766866967067167267367467567667767867968068168268368468568668768868969069169269369469569669769869970070170270370470570670770870971071171271371471571671771871972072172272372472572672772872973073173273373473573673773873974074174274374474574674774874975075175275375475575675775875976076176276376476576676776876977077177277377477577677777877978078178278378478578678778878979079179279379479579679779879980080180280380480580680780880981081181281381481581681781881982082182282382482582682782882983083183283383483583683783883984084184284384484584684784884985085185285385485585685785885986086186286386486586686786886987087187287387487587687787887988088188288388488588688788888989089189289389489589689789889990090190290390490590690790890991091191291391491591691791891992092192292392492592692792892993093193293393493593693793893994094194294394494594694794894995095195295395495595695795895996096196296396496596696796896997097197297397497597697797897998098198298398498598698798898999099199299399499599699799899910001001100210031004100510061007100810091010101110121013101410151016101710181019102010211022102310241025102610271028102910301031103210331034103510361037103810391040104110421043104410451046104710481049105010511052105310541055105610571058105910601061106210631064106510661067106810691070107110721073107410751076107710781079108010811082108310841085108610871088108910901091109210931094109510961097109810991100110111021103110411051106110711081109111011111112111311141115111611171118111911201121112211231124112511261127112811291130113111321133113411351136113711381139114011411142114311441145114611471148114911501151115211531154115511561157115811591160116111621163116411651166116711681169117011711172117311741175117611771178117911801181118211831184118511861187118811891190119111921193119411951196119711981199120012011202120312041205120612071208120912101211121212131214121512161217121812191220122112221223122412251226122712281229123012311232123312341235123612371238123912401241124212431244124512461247124812491250125112521253125412551256125712581259126012611262126312641265126612671268126912701271127212731274127512761277127812791280128112821283128412851286128712881289129012911292129312941295129612971298129913



Microscope

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UNITED STATES OF AMERICA
COMBINED DECLARATION AND POWER OF ATTORNEY
FOR PATENT APPLICATION

FILE NO. GK-ZEI-3049

As a below named inventor, I hereby declare that: my residence, post office address and citizenship are as stated below next to my name; that I verily believe that I am the original, first and sole inventor (if only one name is listed below) or a joint inventor (if plural inventors are named) of the subject matter which is claimed and for which a patent is sought on the invention entitled:

ARRANGEMENT FOR ILLUMINATION AND/OR DETECTION IN A MICROSCOPE

the specification of which

☒ is attached hereto.

☐ was filed on _____ as United States patent application Serial Number _____.

☐ was filed on _____ as PCT international patent application No. _____
and was amended on _____ (if any).

I hereby state that I have reviewed and understand the contents of the above identified specification, including the claims, as amended by any amendment referred to above.

I acknowledge the duty to disclose all information known to be material to patentability in accordance with Title 37, Code of Federal Regulations, §1.56.

I hereby claim foreign priority benefits under Title 35, United States Code §119 of any foreign application(s) for patent or inventor's certificate listed below and have also identified below any foreign application for patent or inventor's certificate having a filing date before that of the application on which priority is claimed:

Prior Foreign Application(s)

COUNTRY	APPLICATION NUMBER	DATE OF FILING (day, month, year)	PRIORITY CLAIMED UNDER 35 U.S.C. 119
Germany	198 35 072.4	04 August 1998	YES <input checked="" type="checkbox"/> NO <input type="checkbox"/>
			YES <input type="checkbox"/> NO <input type="checkbox"/>

I hereby appoint McAULAY NISSEN GOLDBERG KIEL & HAND and the members of the firm: Lloyd McAulay, Reg. No. 20,423; J. Harold Nissen, Reg. No. 17,283; Jules E. Goldberg, Reg. No. 24,408; Gerald H. Kiel, Reg. No. 25,116; Francis C. Hand, Reg. No. 22,280; Eugene LeDonne, Reg. No. 35,930; Mark Montague, Reg. No. 36,612; Stephen Chin, Reg. No. 39,938; Arthur Dresner, Reg. No. 24,403; and F. Aaron Dubberley, Reg. No. 41,001; as attorneys with full power of substitution and revocation to prosecute all business in the Patent & Trademark Office connected therewith and to receive all correspondence.

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I hereby declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under Section 1001 of Title 18 of the United States Code, and that such willful false statements may jeopardize the validity of the application or any patent issued thereon.

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COMBINED DECLARATION AND POWER OF ATTORNEY FOR PATENT APPLICATION (continued)		File No. GK-ZEI-3049	
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POST OFFICE ADDRESS			
FULL NAME OF SEVENTH JOINT INVENTOR (IF ANY)		INVENTOR'S SIGNATURE	DATE
RESIDENCE		COUNTRY OF CITIZENSHIP	
POST OFFICE ADDRESS			
FULL NAME OF EIGHTH JOINT INVENTOR (IF ANY)		INVENTOR'S SIGNATURE	DATE
RESIDENCE		COUNTRY OF CITIZENSHIP	
POST OFFICE ADDRESS			
FULL NAME OF NINTH JOINT INVENTOR (IF ANY)		INVENTOR'S SIGNATURE	DATE
RESIDENCE		COUNTRY OF CITIZENSHIP	
POST OFFICE ADDRESS			